

# Catching Physiological Noise: Comparison of DRIFTER in Image and $k$ -Space

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## INTRODUCTION

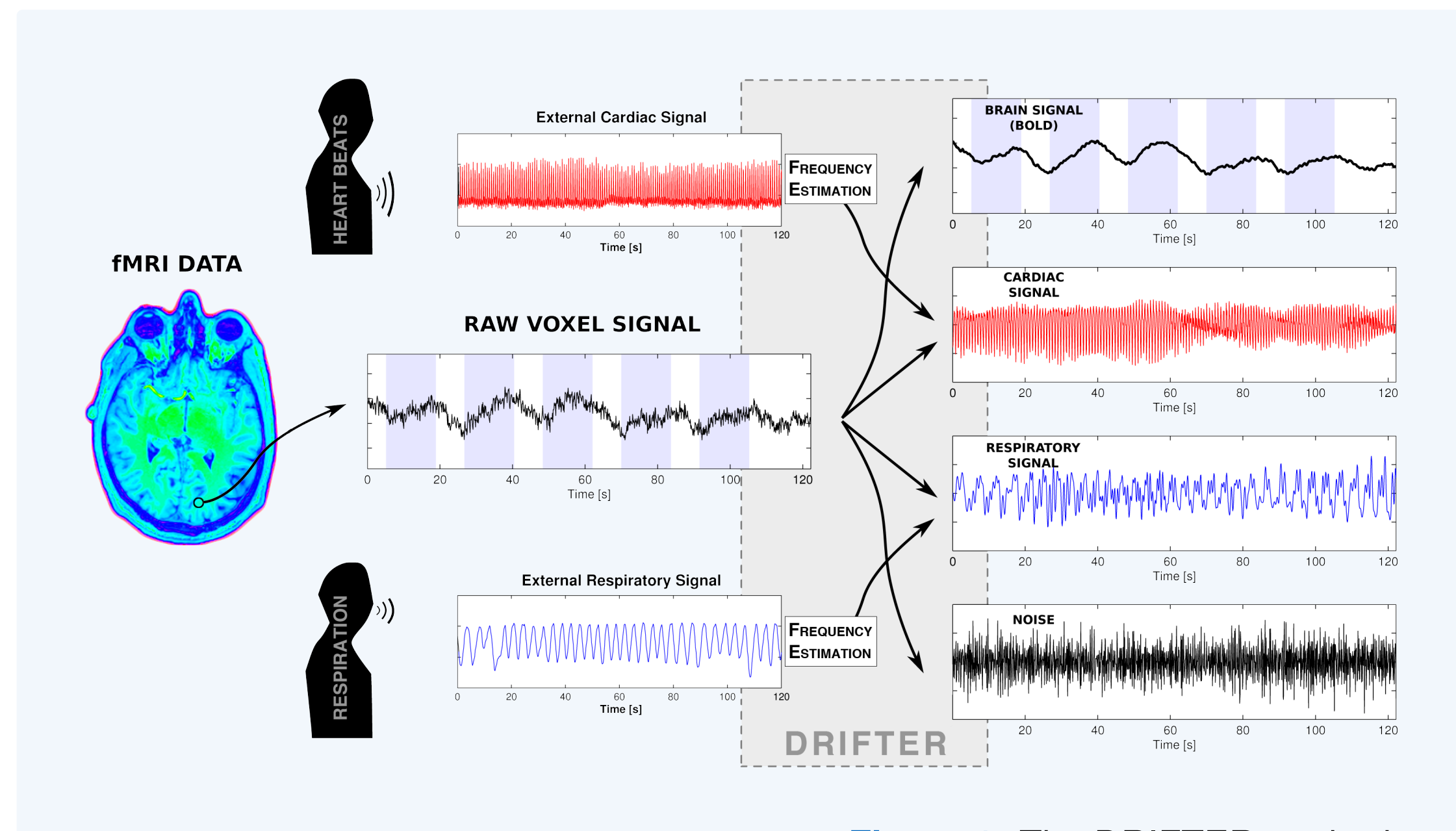
- ▶ We aim to **improve the signal-to-noise ratio (SNR)** of fMRI through accurate treatment of non-white noises.
- ▶ The non-white noise is mainly induced by **heartbeat, respiration, and variation in blood flow** [1].
- ▶ Such structural noise is usually removed by retrospective methods [2, 3] using only the reconstructed magnitude images.
- ▶ We show how the DRIFTER [3] method can be extended to work with both  **$k$ -space and complex image space data**.
- ▶ The results show that it is beneficial to remove the noise components already **prior to reconstructing the magnitude images**.

## DRIFTER

- ▶ DRIFTER [3] is a model-based method for retrospective estimation and removal of physiological noise.
- ▶ The method uses Bayesian optimal filtering methods, and it has shown **excellent performance** in comparison to other methods.
- ▶ DRIFTER combines information from fast-sampled physiological reference signals with the data to separate the noise.
- ▶ Decomposing the fMRI data into additive components:
  - (1) Oscillatory structured noises
  - (2) Slow drift and the BOLD signal
  - (3) Unstructured residuals
- ▶ The idea is visualized in Figure 1.

## MATERIAL

- ▶ A 27-run set of **resting state fMRI** data and **anatomical images** for one volunteer obtained with a 3 T scanner (Siemens Skyra; 32-channel coil array).
- ▶ EPI sequence parameters: TR: 77 ms; TE: 21 ms; FA: 60°; FOV: 224 mm; matrix size: 64×64; and voxel size: 3.5×3.5×6 mm.
- ▶ EPI trajectory parameters: ramp times: 140  $\mu$ s, flat-top time: 220  $\mu$ s, and ADC readout time: 409.6  $\mu$ s.
- ▶ **Cardiac and respiration reference signals** time-locked to the fMRI data using peripheral pulse measure and a respiratory belt.
- ▶ We used two harmonic resonators in the DRIFTER algorithm.



**Figure 1:** The DRIFTER method for separation of physiological noise in fMRI data. Each voxel time series is dealt with independently.

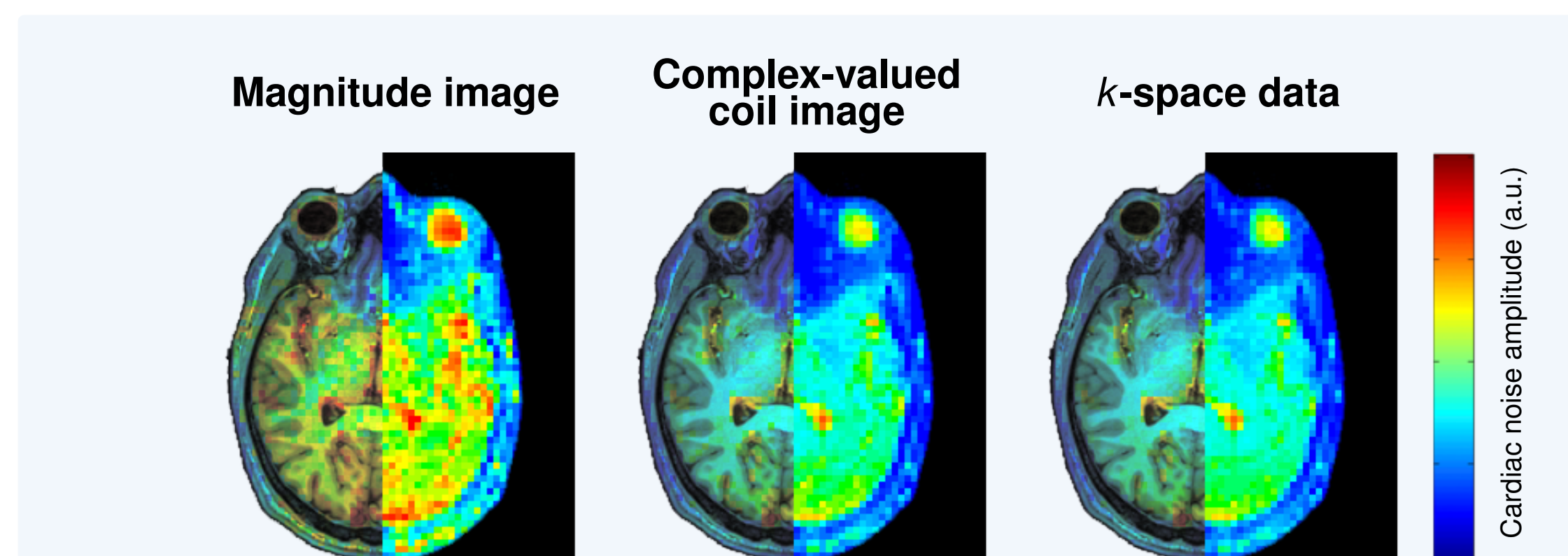
## METHODS

- ▶ We apply the DRIFTER method to:
  - (1) Magnitude images (standard sum-of-squares reconstruction)
  - (2) Complex-valued reconstructed coil images
  - (3) Raw  $k$ -space data before reconstruction
- ▶ In the complex-valued data, the real and imaginary components were dealt with independently.
- ▶ We used Kaiser–Bessel regridding [4, 5] in the reconstruction.
- ▶ The final maps for the complex and  $k$ -space data were weighted by the coil images when summing over the channels (as in sum-of-squares reconstruction).
- ▶ Amplitude maps are compared against the anatomical image.
- ▶ This analysis is done for each set of data/slice independently.

The DRIFTER toolbox for Matlab/SPM is available online: <http://becs.aalto.fi/en/research/bayes/drifter/>

## RESULTS

- ▶ In Figure 2, we show cardiac noise amplitude maps for a set of slices and separated at different stages of the reconstruction.
- ▶ The comparison of the complex and magnitude image space data DRIFTER deals with each voxel spatially independently, whereas in the  $k$ -space data, DRIFTER is independent over the  $k$ -space.
- ▶ The results show differences in the spatial localization of the noise.



**Figure 2:** Cardiac noise amplitude maps (slice 14) reconstructed from the magnitude image data and compared to maps from complex coil image data, and  $k$ -space data. The noise magnitudes are logarithmic and may vary between the methods.

## DISCUSSION

- ▶ The overall map structures agree with earlier results [6].
- ▶ The results should in theory be similar, as the components in DRIFTER are **purely additive** and the inverse Fourier transform reconstruction is a **linear operation**.
- ▶ However, there are **clear differences** in the noise reconstruction between the magnitude images, and the complex image and  $k$ -space data.
- ▶ The latter ones are almost identical, the slight differences stem from the **non-uniform sampling** of the  $k$ -space.
- ▶ The results imply that the noise influence is clearly **more localized in the complex and  $k$ -space maps**, especially near the big arterial veins.
- ▶ Estimation of the structured physiological noise should be done **before the noise effects get aliased** into the image data.

## CONCLUSION

- ▶ We have presented how the physiological noise removal method DRIFTER can be **applied to complex-valued fMRI image data and raw  $k$ -space data**.
- ▶ The findings motivate further development of tools for catching physiological noise.
- ▶ The DRIFTER toolbox for SPM8 and Matlab is available for download online.

## REFERENCES

- [1] Triantafyllou C., Hoge R.D., Krüger G. Comparison of physiological noise at 1.5 T, 3 T and 7 T and optimization of fMRI acquisition parameters. *NeuroImage*. 2005;26(1):243–250.
- [2] Glover G.H., Li T.Q., Ress D. Image-based method for retrospective correction of physiological motion effects in fMRI: RETROICOR. *MRM*. 2000;44(1):162–167.
- [3] Särkkä S., Solin A., Nummenmaa A., et al. Dynamical retrospective filtering of physiological noise in BOLD fMRI: DRIFTER. *NeuroImage*. 2012;60(2):1517–1527.
- [4] Beatty P.J., Nishimura D.G., Pauly, J.M. Rapid gridding reconstruction with a minimal oversampling ratio. *IEEE T Med Imaging*. 2005;24(6):799–808.
- [5] Bernstein M.A., King K.F., Zhou X.J. *Handbook of MRI Pulse Sequences*. Academic Press, Amsterdam. 2004.
- [6] Särkkä S., Solin A., Nummenmaa A., et al. Identification of spatio-temporal oscillatory signal structure in cerebral hemodynamics using DRIFTER. *Proc. of ISMRM 2012*;20:2842.

